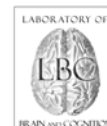


Multi-echo EPI for resting state and activation-based fMRI

Javier González-Castillo

Section on Functional Imaging Methods, NIMH, NIH

March 24th, 2016. Texas Tech Neuroimaging Institute, Lubbock, TX.





- *Noise sources in fMRI*
- *Multi-echo fMRI as a Denoising Technique*
- *ME-ICA Denoising*
- *ME-ICA Denoising Applications*
- *Conclusions*

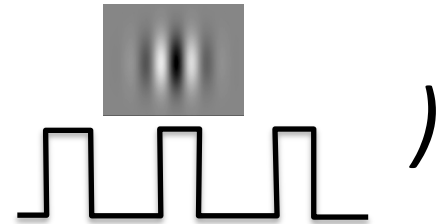
$fMRI = f($



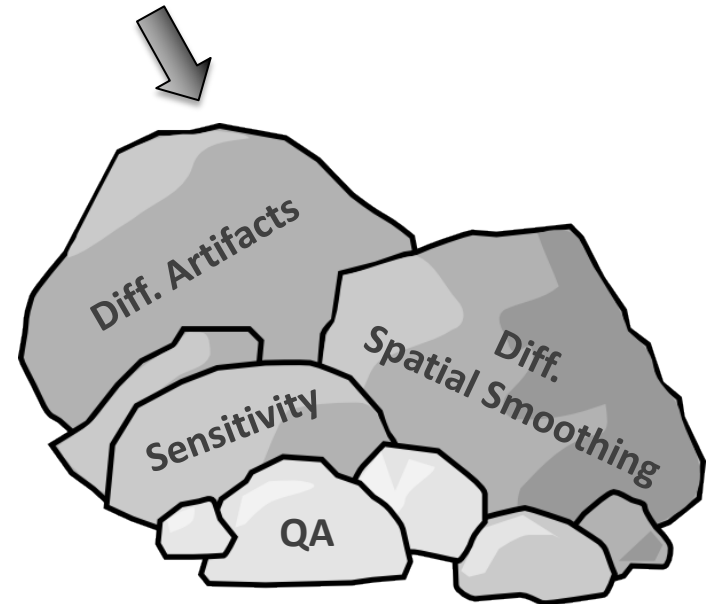
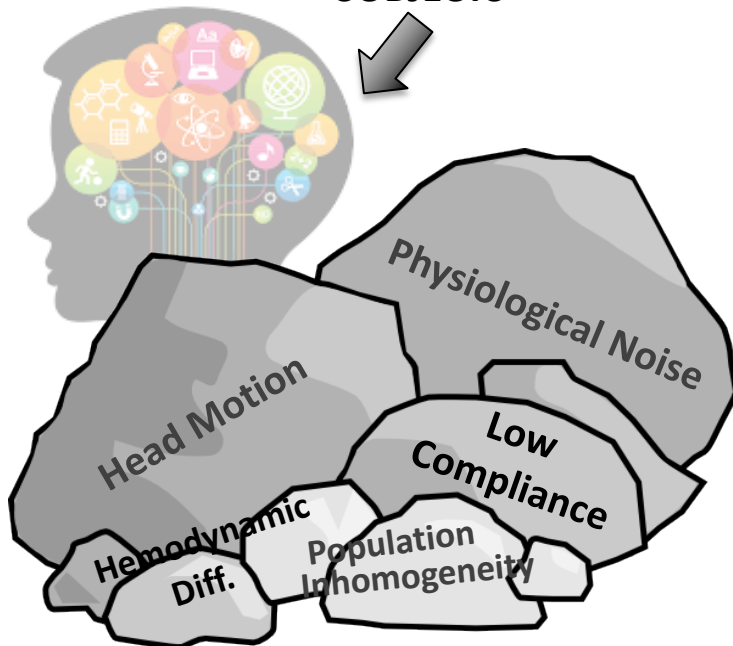
SUBJECTS



HW
(SCANNER)



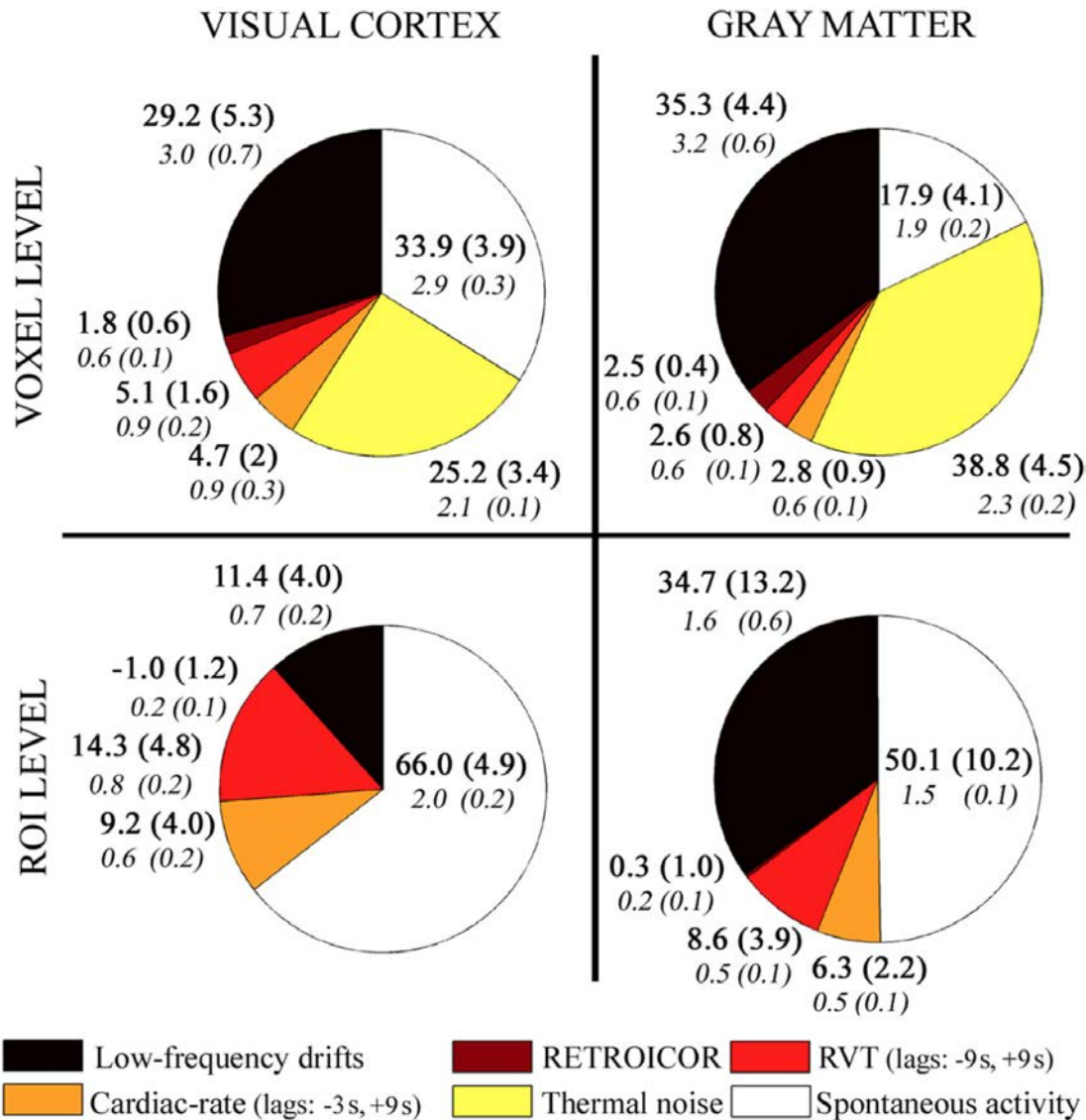
EXPERIMENTAL
PARADIGM

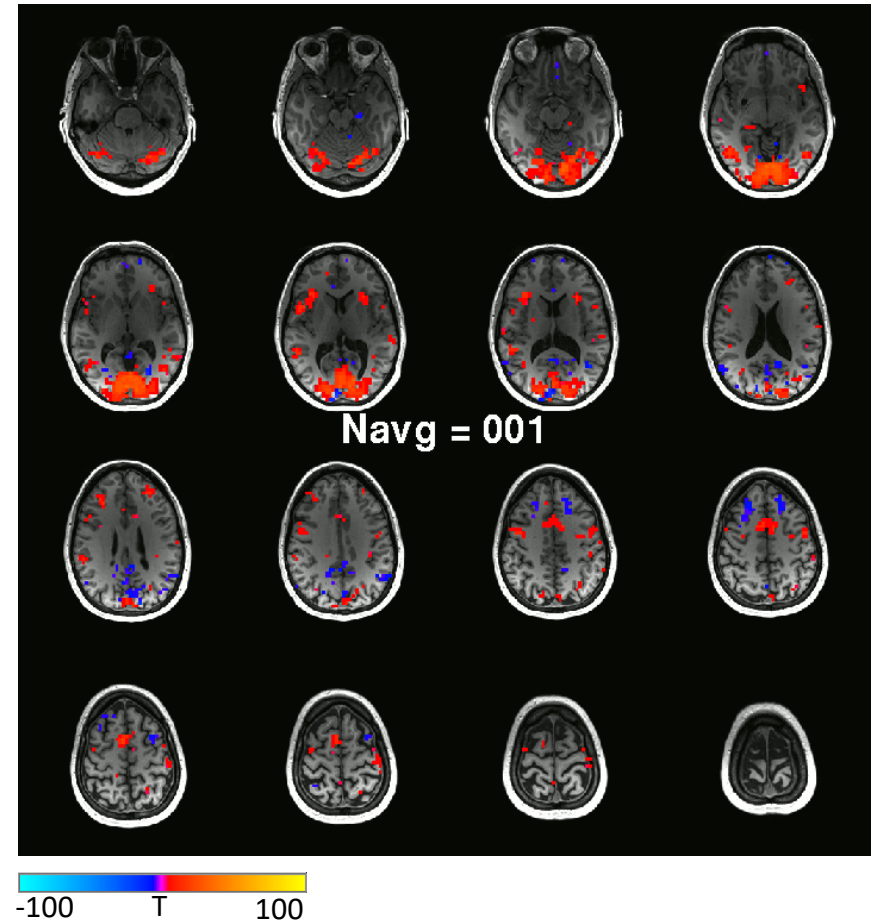
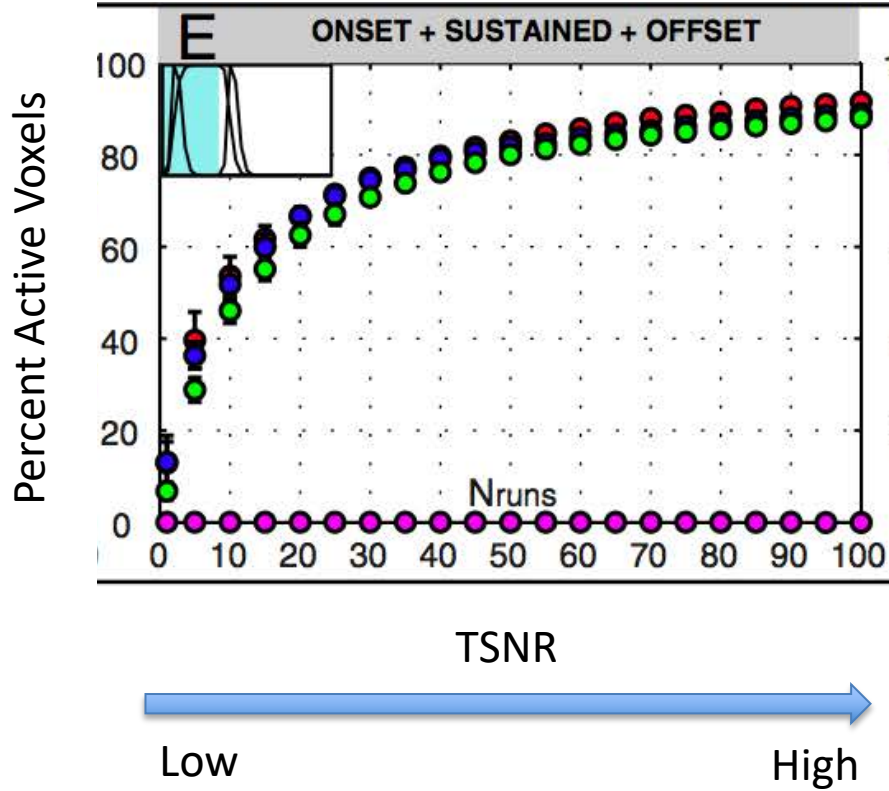


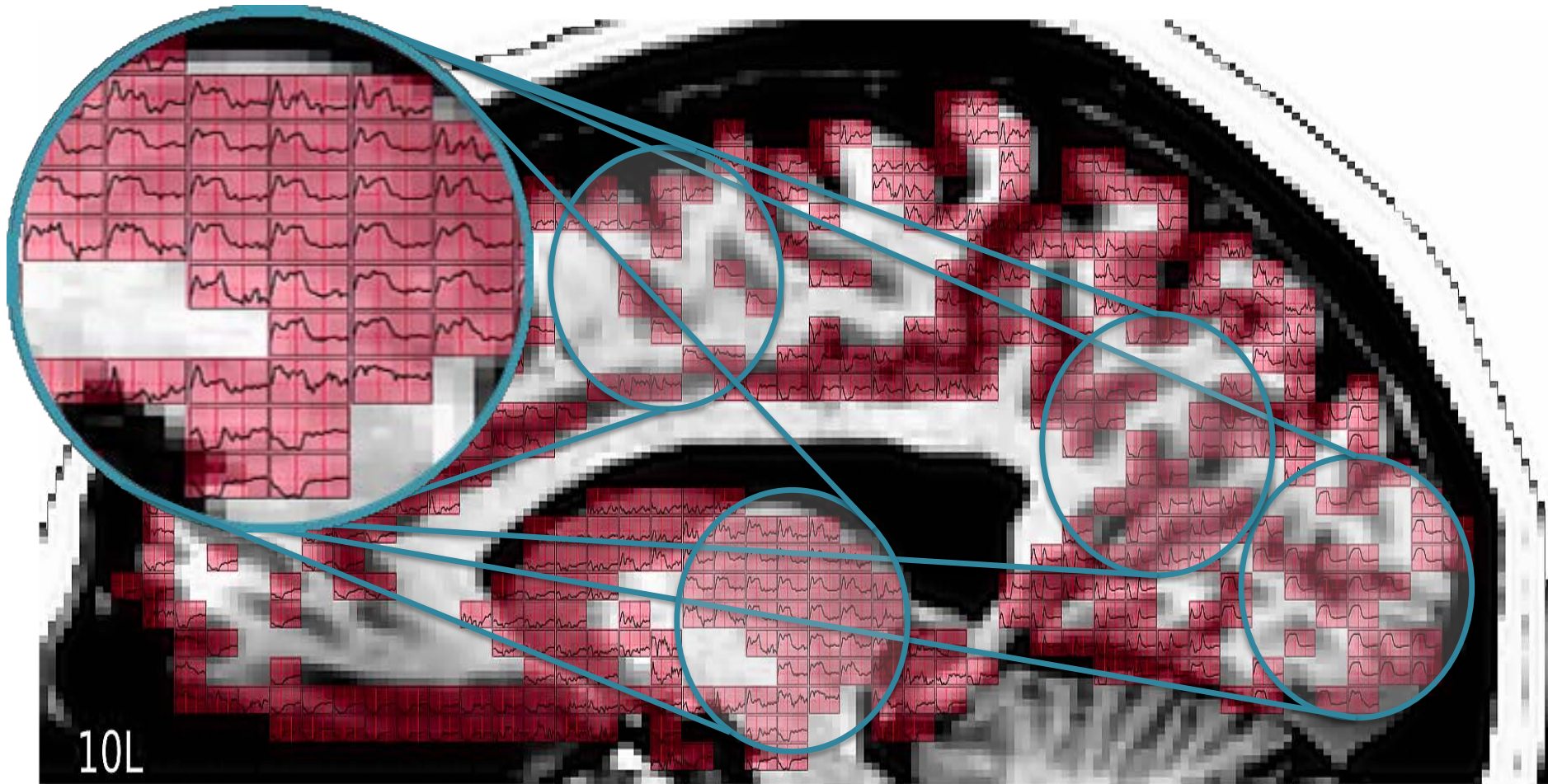
ONLY A SUBSET OF THE SIGNAL WE MEASURE CONTAIN INFORMATION ABOUT NEURONAL PROCESSES

How to best isolate and interpret this extremely valuable component of the fMRI signal?

fMRI Time series = **Signal of Interest (NEURONAL ORIGIN)** + **Other Fluctuations**







10L

NOISE SOURCE



Slow Signal Drifts



Head Motion



Physiological Noise

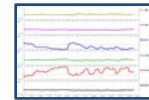


Localized HW Instabilities

MODEL REGRESSOR



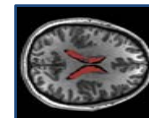
Legendre Polynomials



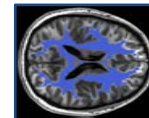
Head Motion Estimates



RETROICOR + RVT



Lateral Ventricle Regressors



Local WM Regressor

MEICA is not only a pre-processing technique, it also requires data to be acquired differently.

1

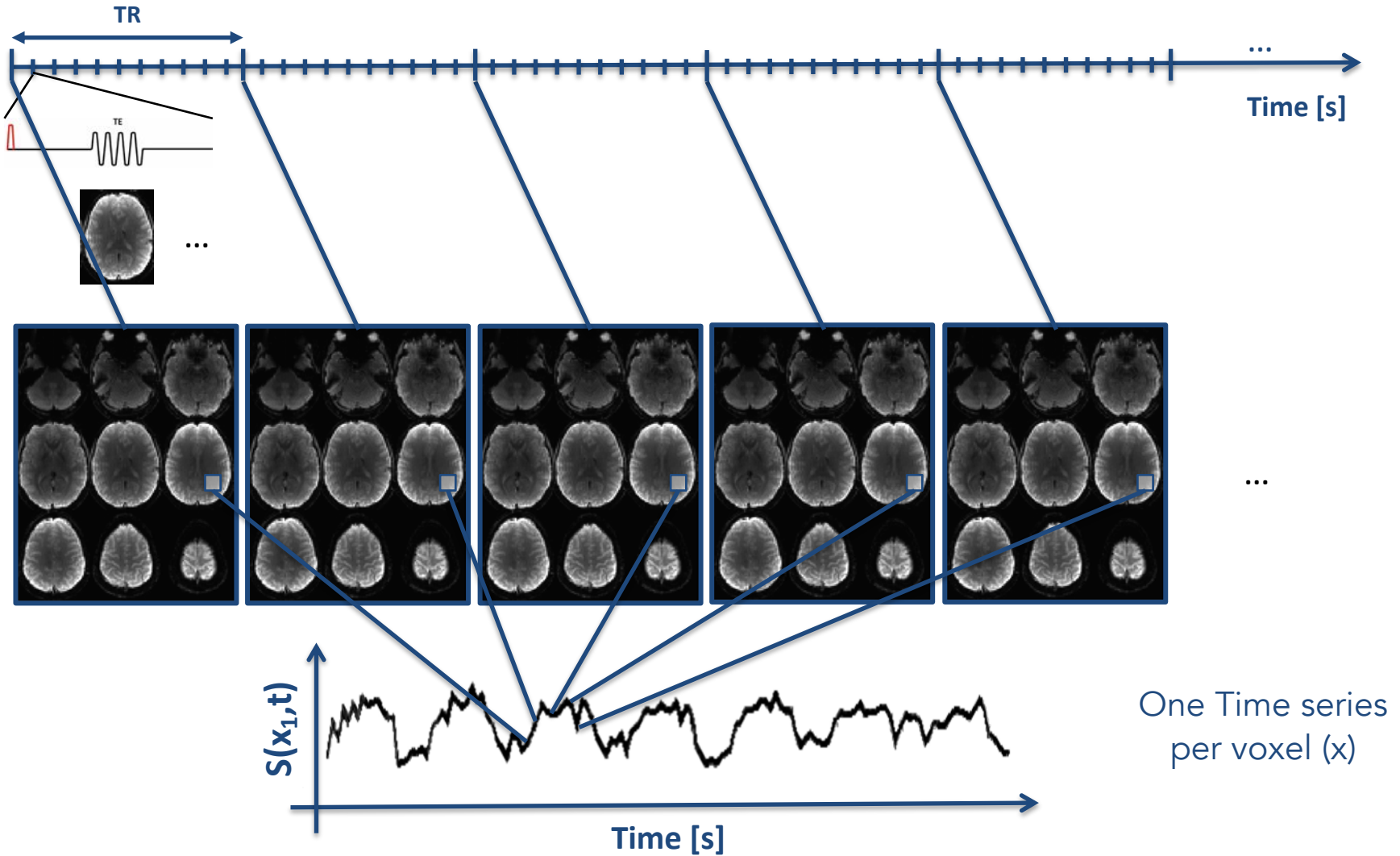
MULTI-ECHO DATA
ACQUISITION

2

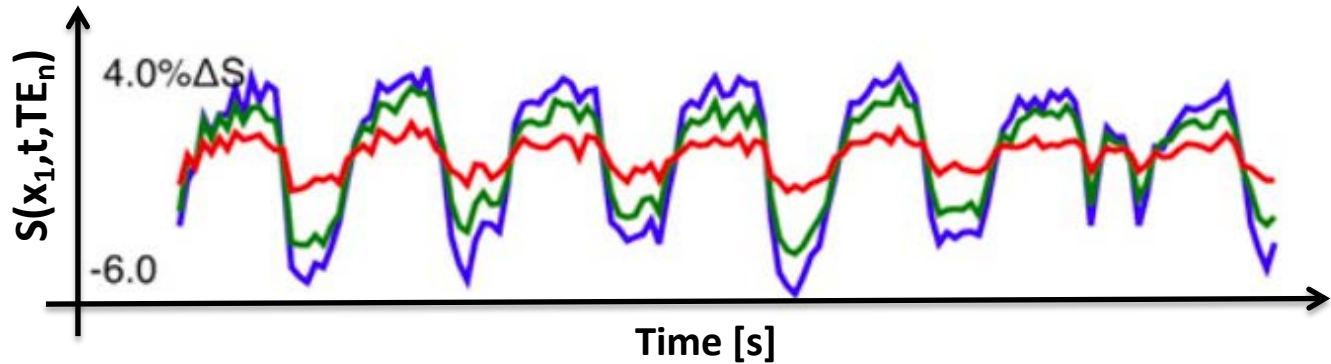
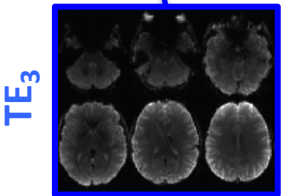
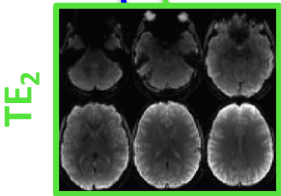
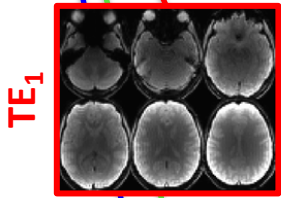
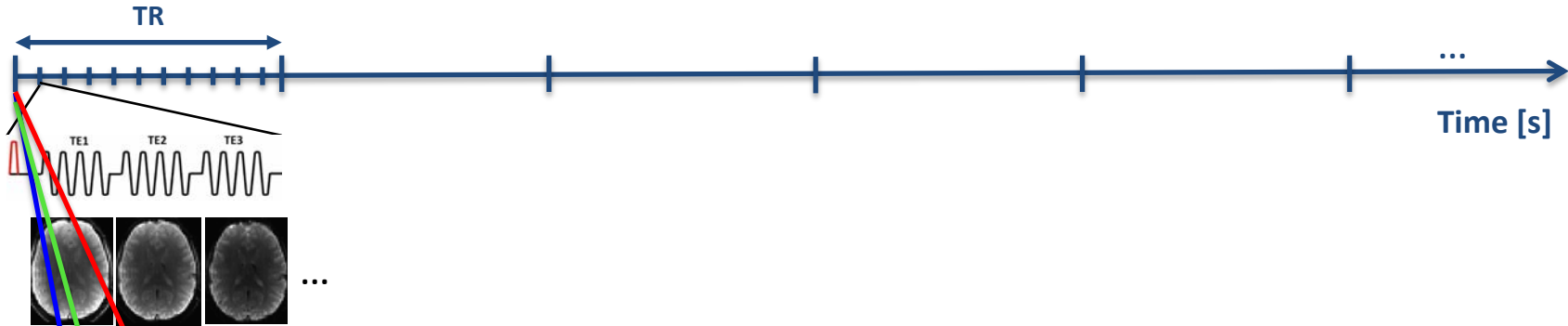
ICA DECOMPOSITION TO OBTAIN
SPATIALLY INDEPENDENT SOURCES
OF FLUCTUATION IN THE DATA

3

AUTOMATIC CLASSIFICATION OF ICA
COMPONENTS INTO "GOOD OR BAD"
BASED ON A PHYSICALLY INFORMED ECHO-
DEPENDENCE MODEL OF THE SIGNALS

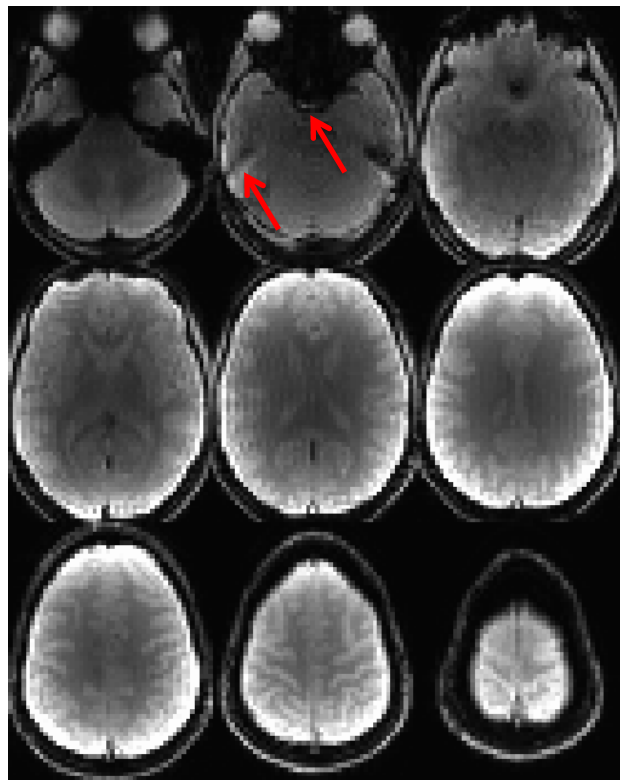
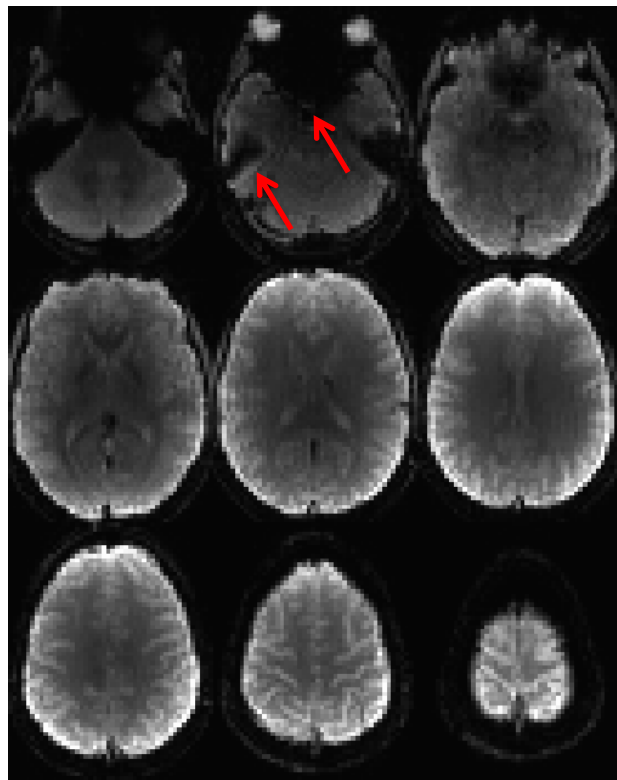
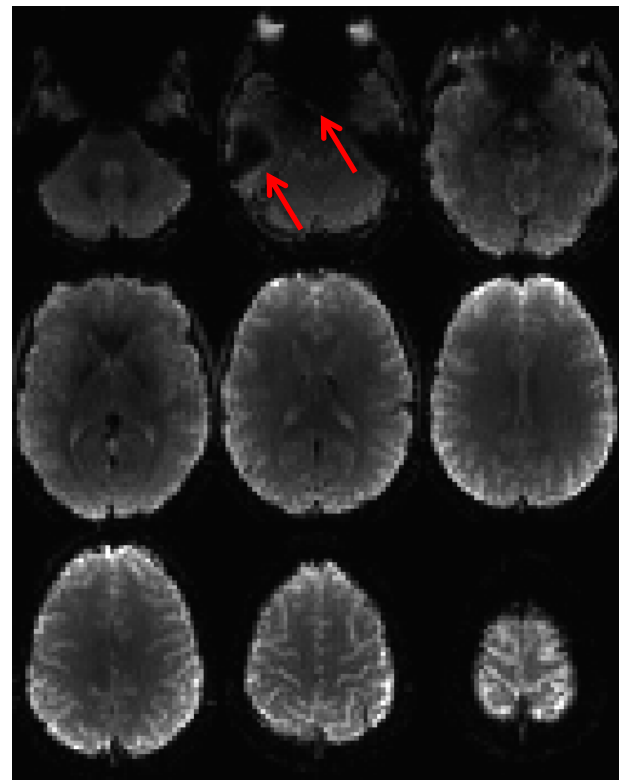


MULTI-ECHO FMRI



Now you have N_e time series per voxel, one per echo time (TE_n):

- No SAR cost, as there are not additional excitation pulses.
- Slight lost in temporal resolution to fit the third echo.
- Slight lost in spatial resolution to make sure you have signal in last echo.

TE_1  TE_2  TE_3 

16

907

16

907

16

907

We have N_e pseudo-concurrent measurements \rightarrow why not simply combine them to reduce uncorrelated white noise present in each individual measurement?

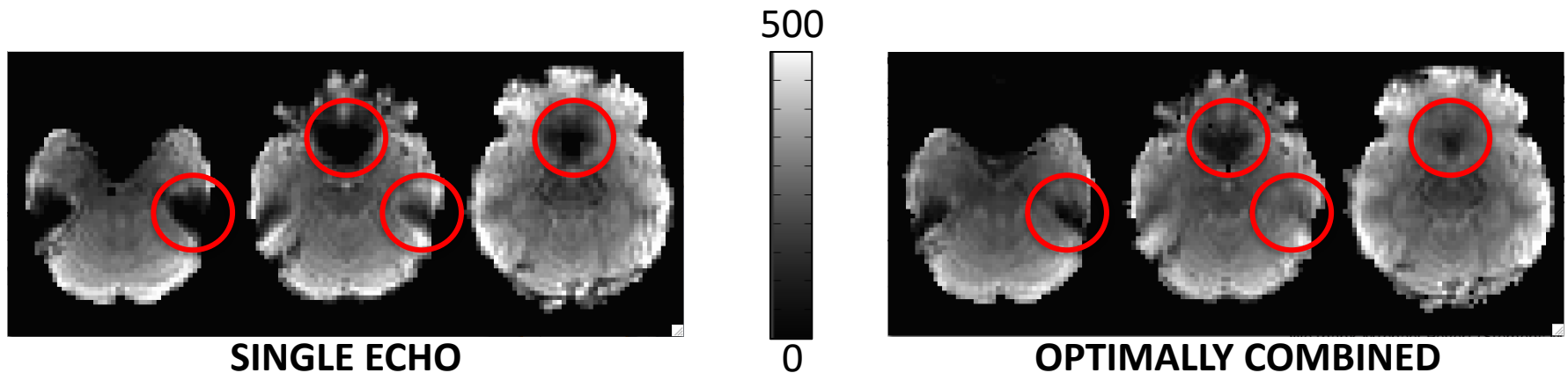
Weighted Summation

$$\hat{S}(x,t) = \sum_{n=1}^N S(x,t,TE_n) \cdot w_v(TE_n)$$

$$w_v(TE_n) = \frac{TE_n e^{-TE_n/T_{2,v}^*}}{\sum_n TE_n \cdot e^{-TE_n/T_{2,v}^*}}$$

- Helps to spatially maximize CNR and also to recover some signal level in regions affected by drop-out.

Posse et al., MRM 1999

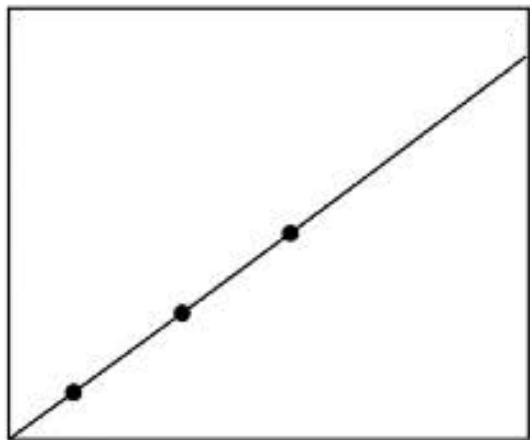


fMRI Data = BOLD-Like Components + Non-BOLD-Like Components

(Neuronal Origin)

(Nuisance/Artifacts)

$\Delta S(x,TE)/S(x,t,TE)$



Echo Time

BOLD-Like Components have a linear dependence with echo time, in terms of signal percent change.

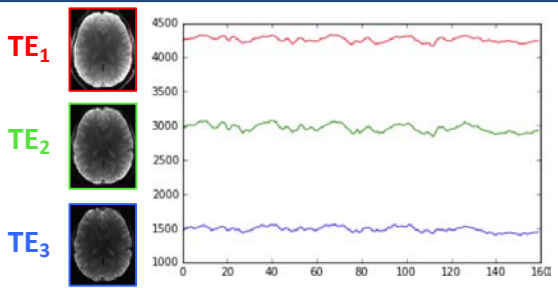
$\Delta S(x,TE)/S(x,t,TE)$



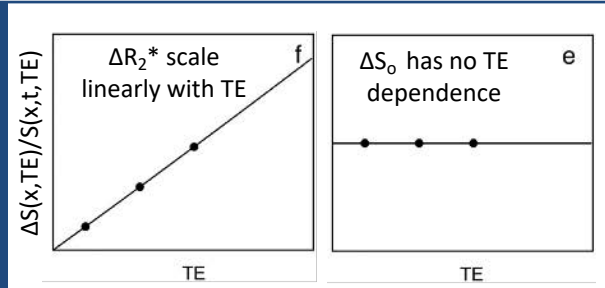
Echo Time

Non-BOLD-Like Components are independent of echo time, in terms of signal percent change

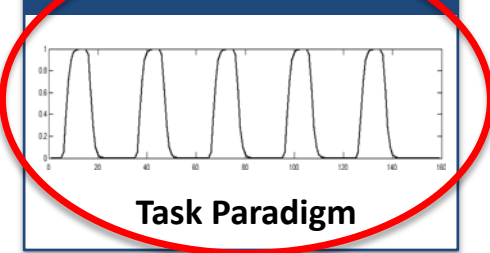
MULTI-ECHO DATASET



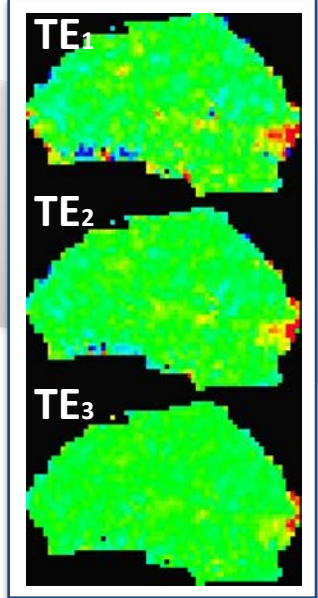
TE-DEPENDENCE MODEL



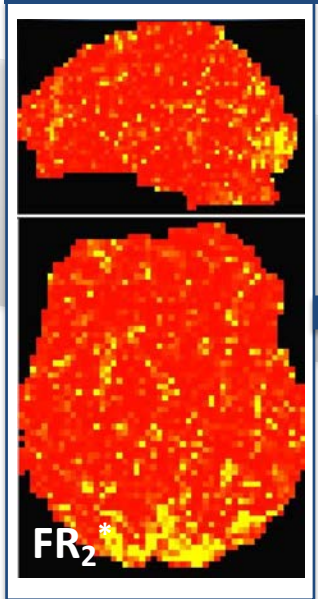
TIMESERIES OF INTEREST



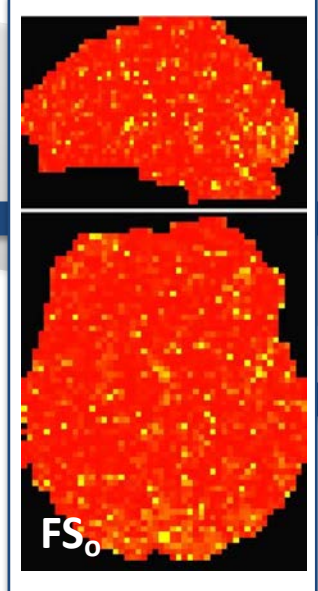
[1] Voxel-wise Fit against all TEs



[2] Voxel-wise Goodness of Fit to R2* Model



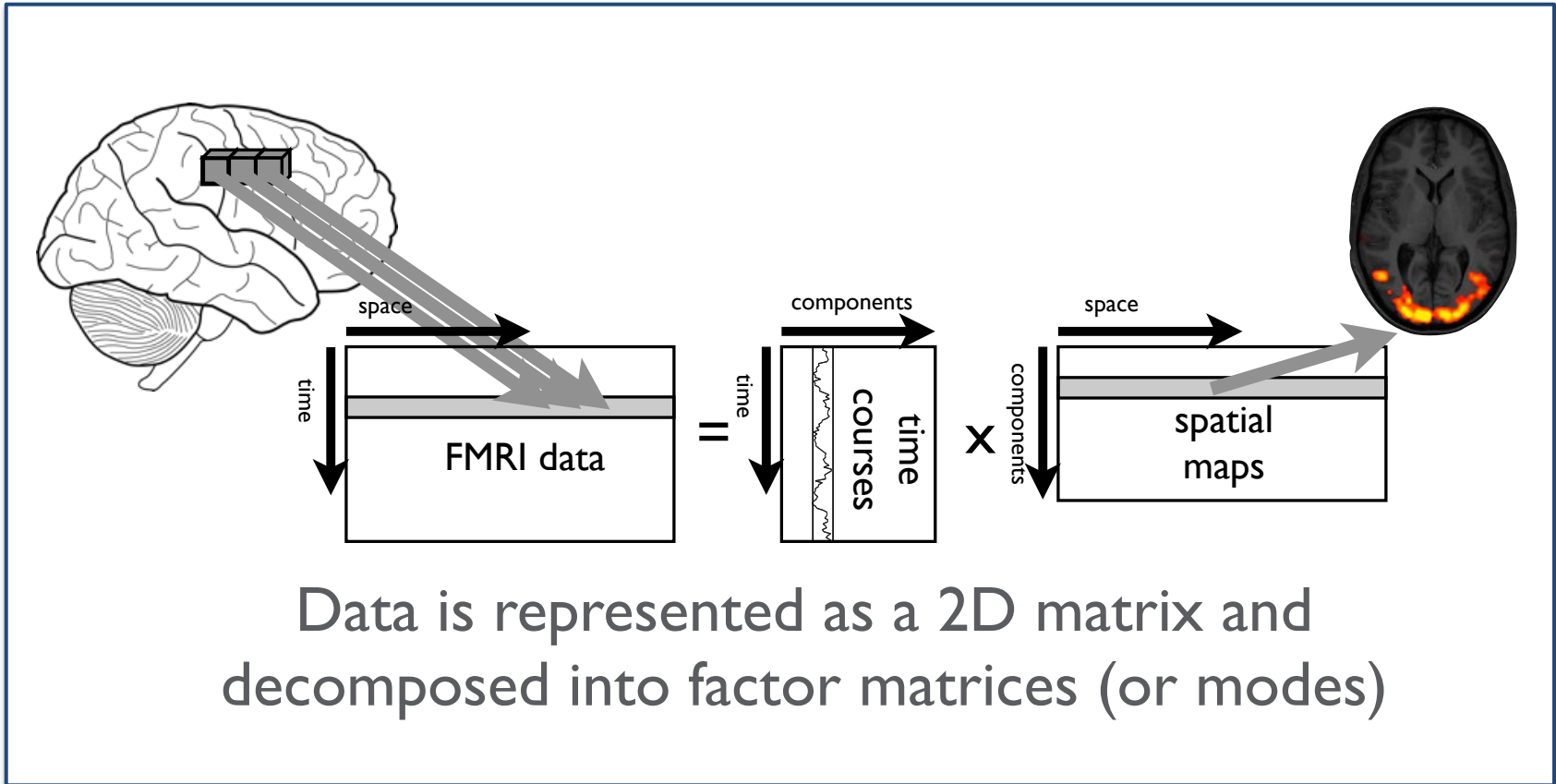
[3] Voxel-wise Goodness of Fit to S0 Model



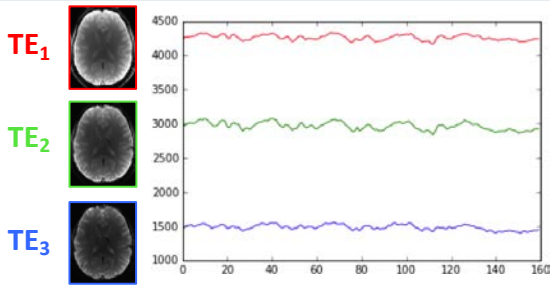
[4] Compute Avg. Metric for each model

$$\kappa = \frac{\sum_{AllVoxels} z_v^2 F_{v,R_2^*}}{\sum_{AllVoxels} z_v^2} = 98.41$$

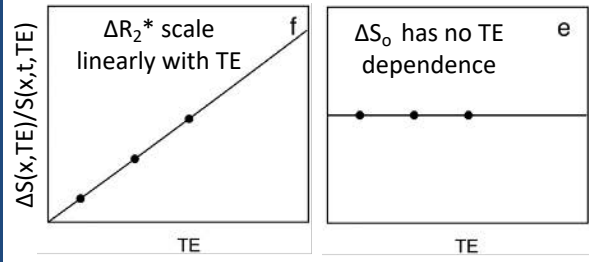
$$\rho = \frac{\sum_{AllVoxels} z_v^2 F_{v,S_0}}{\sum_{AllVoxels} z_v^2} = 26.02$$



MULTI-ECHO
DATASET



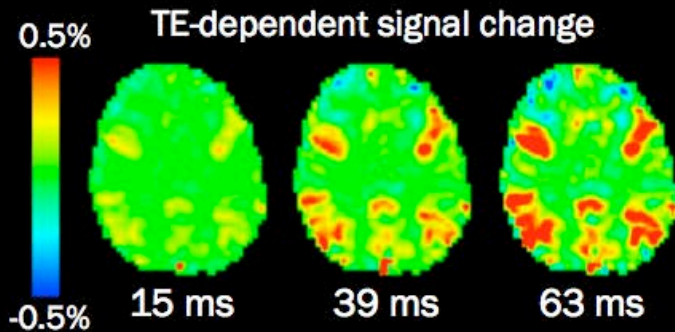
TE-DEPENDENCE
MODEL



ICA TIMESERIES



(a) Functional Network Component



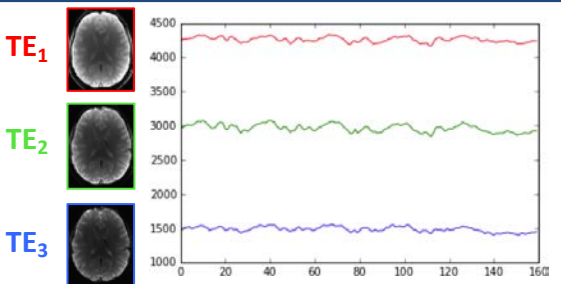
Component time course



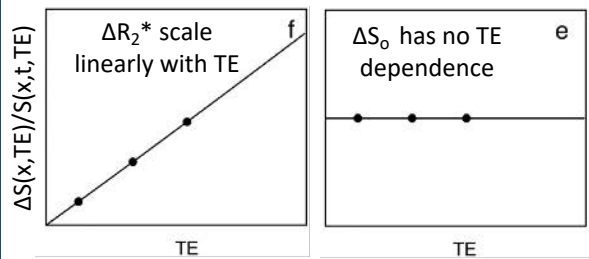
Kappa (κ) = 210

Rho (ρ) = 10

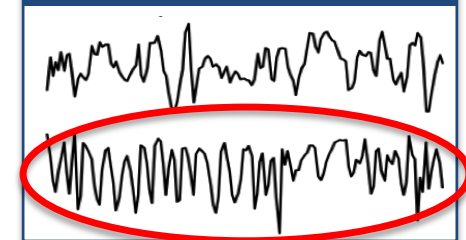
MULTI-ECHO
DATASET



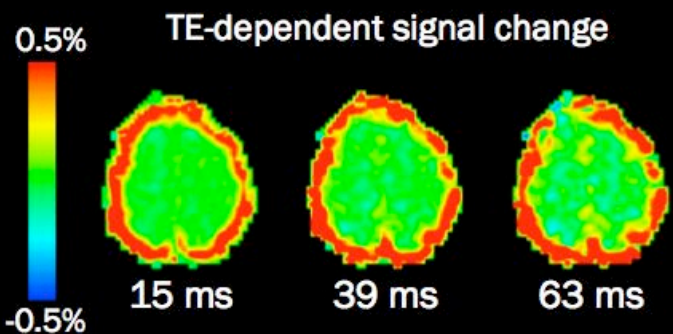
TE-DEPENDENCE
MODEL



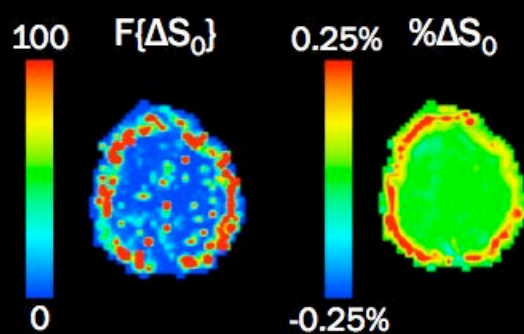
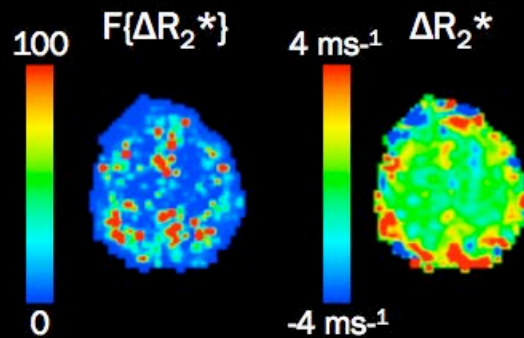
ICA TIMESERIES



(b) Artifact Component

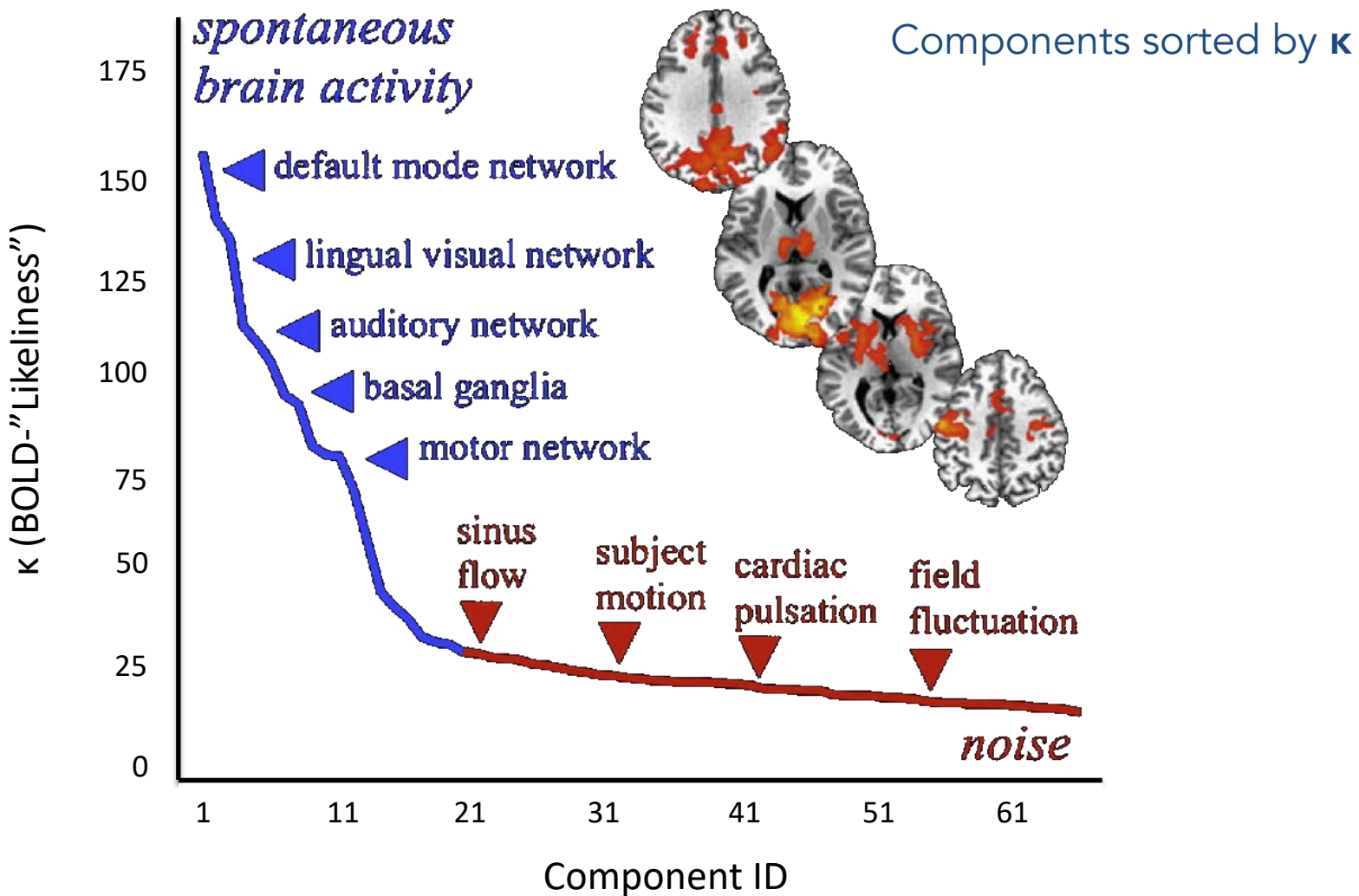


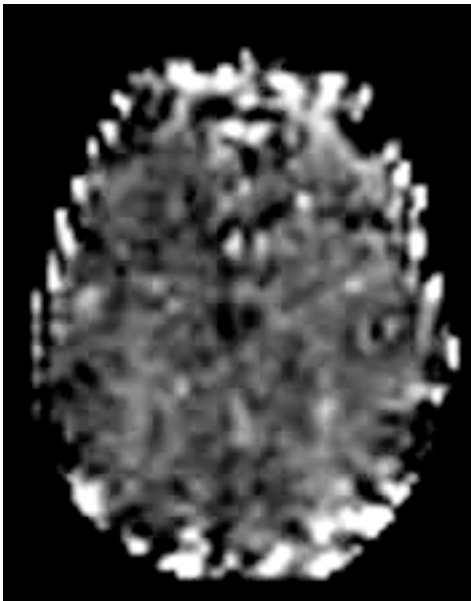
Component time course



Kappa (κ) = 32

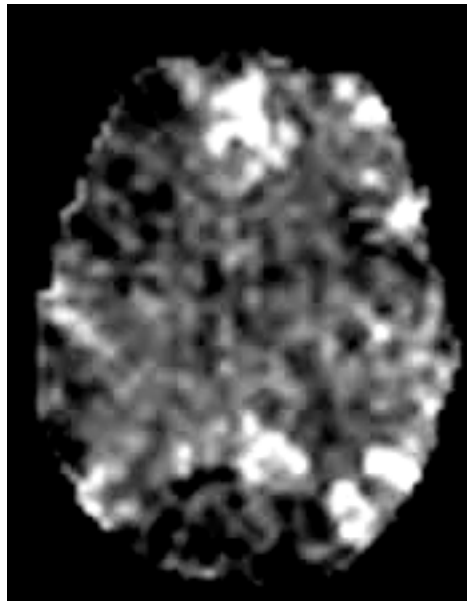
Rho (ρ) = 81





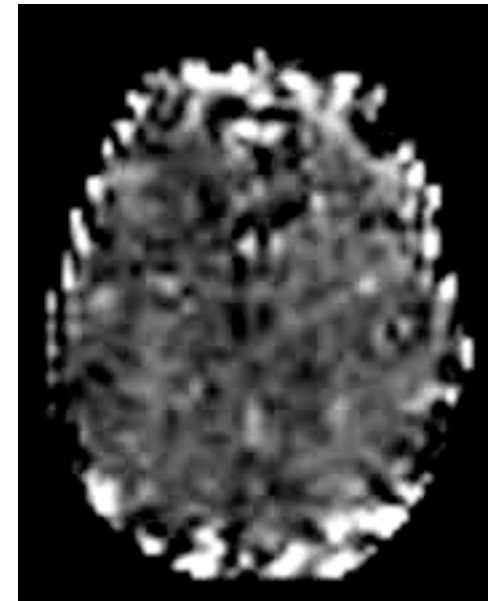
fMRI Timeseries

=



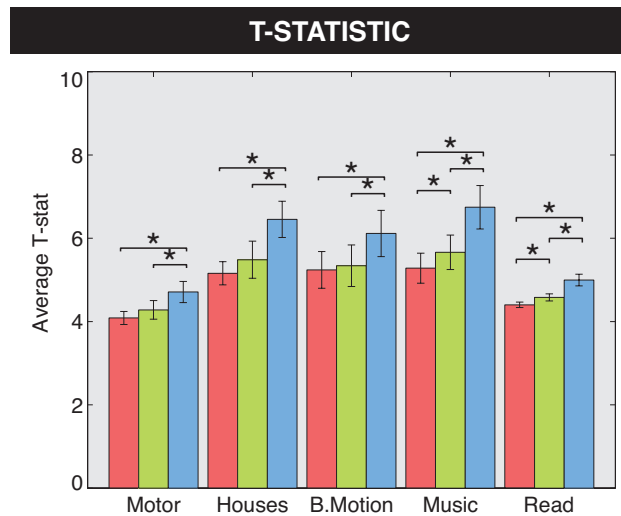
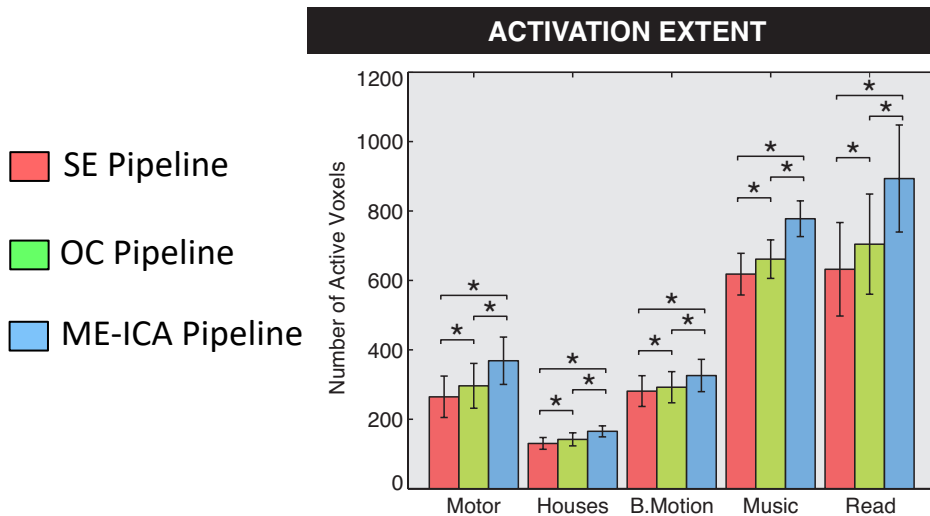
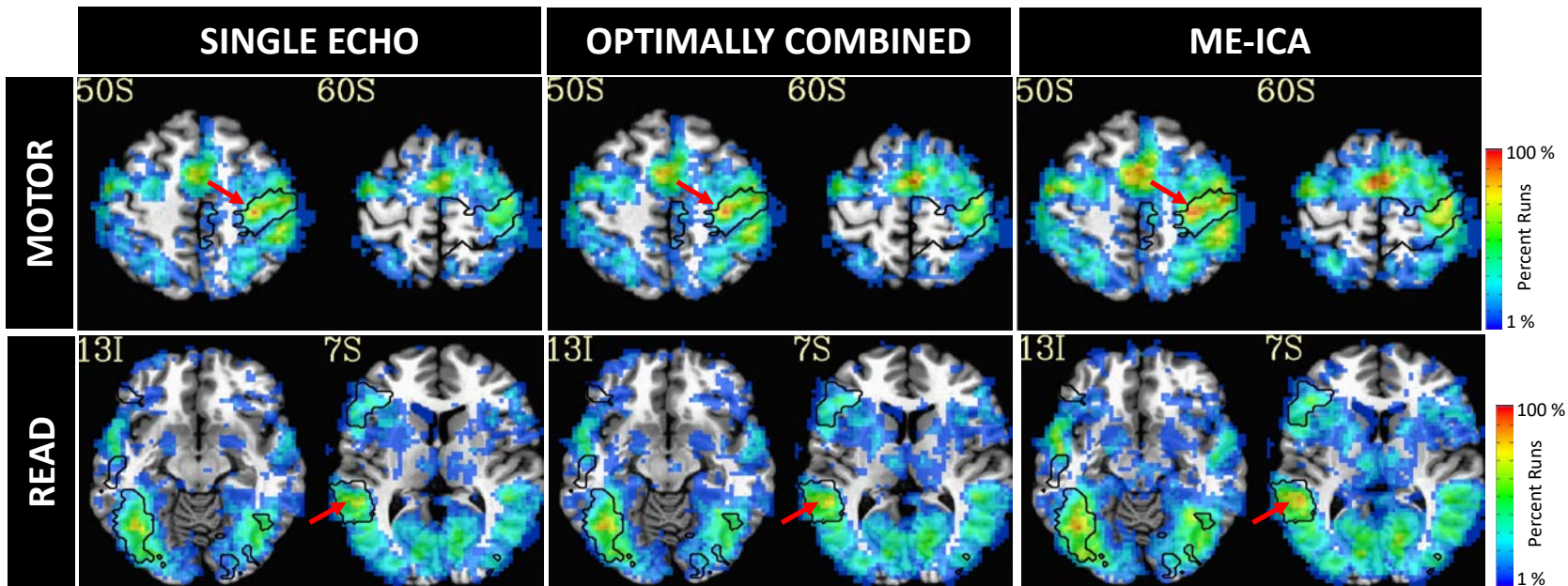
BOLD

+



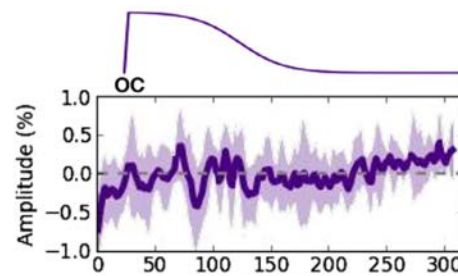
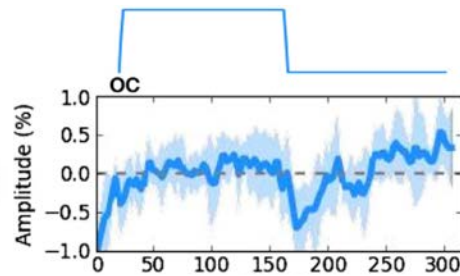
NON BOLD

Multi-Echo fMRI – Improvements for task-based data



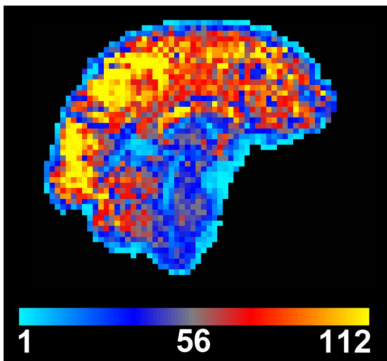
Detection of activity in very slow paradigms (2 min long blocks)

OC

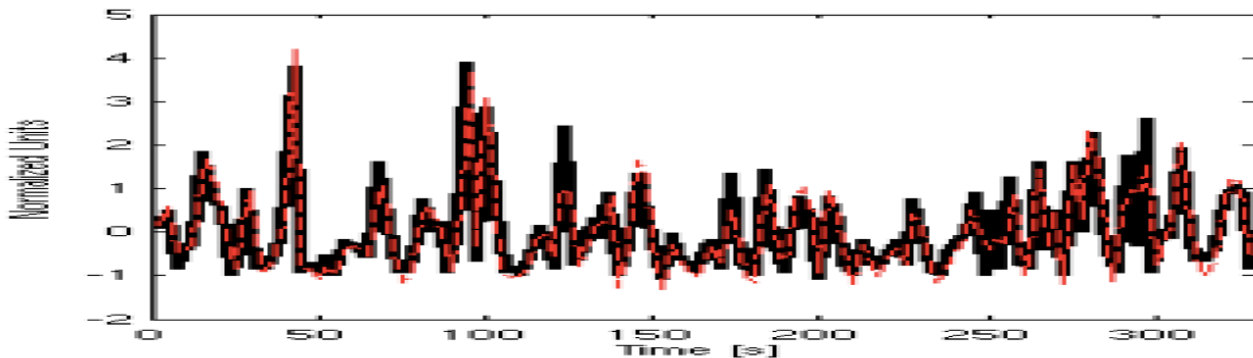
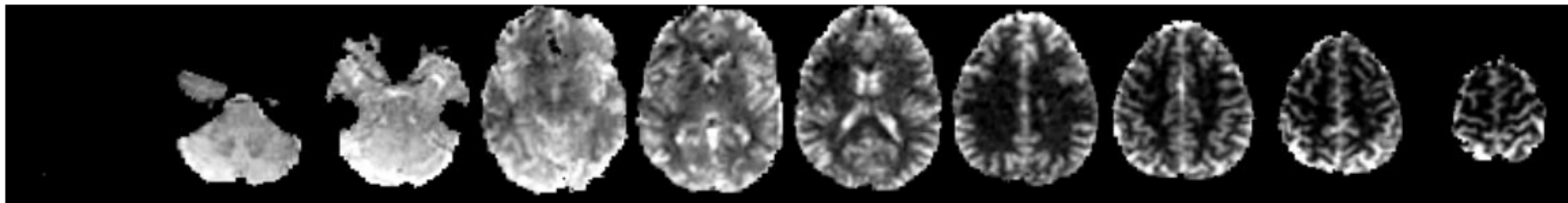
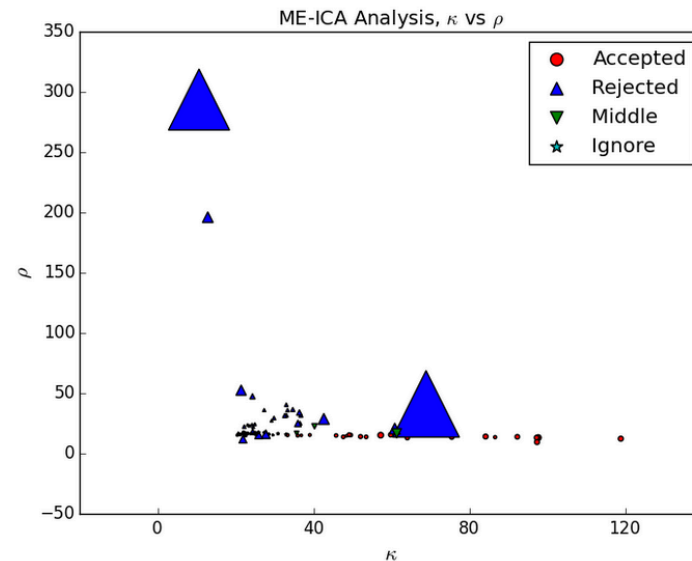
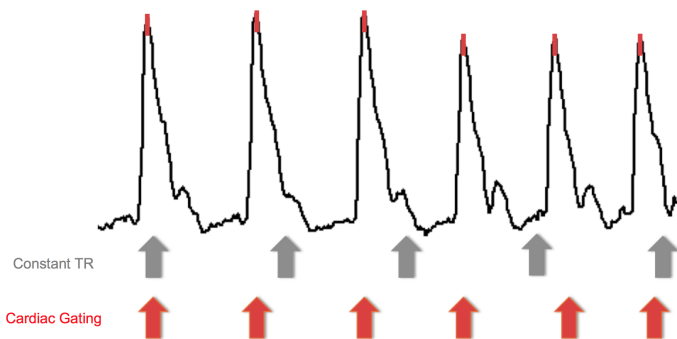


OC



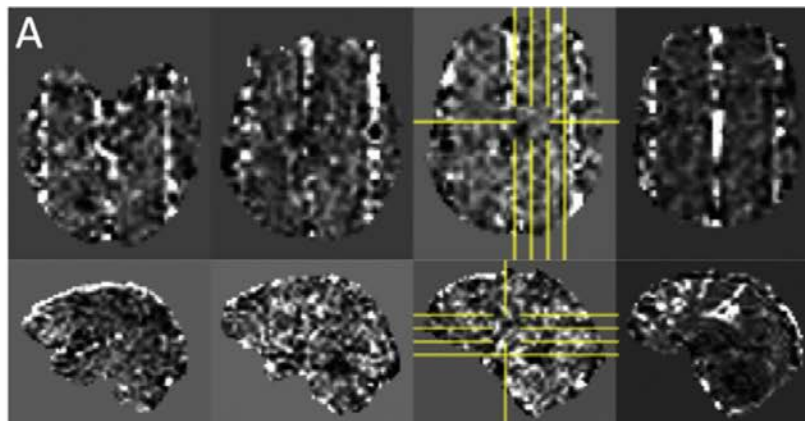


Brooks et al. 2014

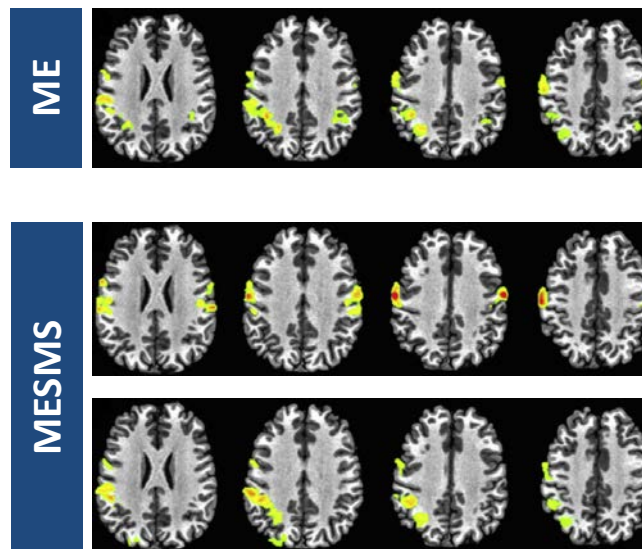
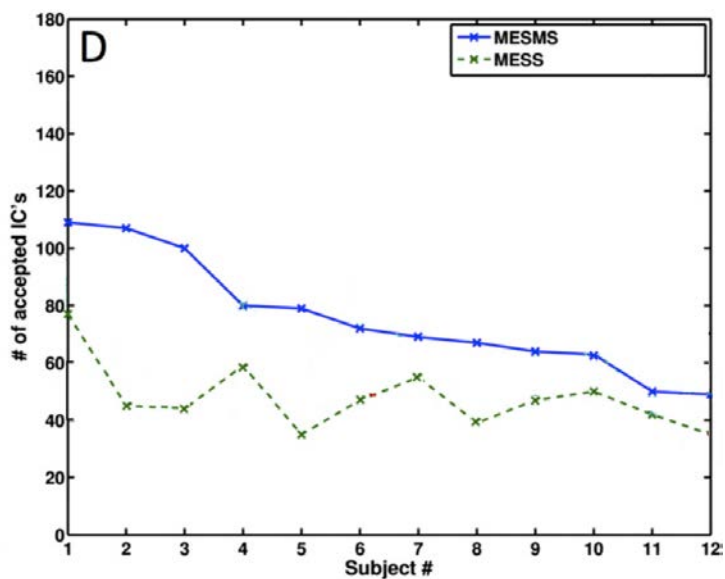


--- Component TS

— ΔTR



Non-BOLD Component: MSS Artifact



Number of BOLD-like components significantly larger for MESMS



- ❑ Multi-echo fMRI allows to capture additional information with minimal costs in terms of temporal and spatial resolution.

- ❑ Such additional information can be used to:
 - ❑ Increase CNR in drop-out regions (e.g., Optimal Combination of Echoes).

 - ❑ Automatically separate BOLD-like from Non-BOLD-like components (ME-ICA).

- ❑ ME-ICA is a promising denoising methodology that combines ICA with TE-Dependence Analysis:
 - ❑ Can substantially improve the SNR of the data → Quality of the results.

 - ❑ Still under development.

Section on Functional Imaging Methods

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 Meghan Robinson
 Colin Hoy
 Laura Buchanan
 Adam Thomas
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Robert W. Cox
 Ziad S. Saad
 Daniel Glen
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Advanced MRI

Catie Chang



Functional MRI Facility

Sean Marrett
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 Souheil Inati
 Andy Derbyshire

